

Abstract

20

21 **Background:** Muscle strength imbalance assessment (e.g. hamstring-to-quadriceps ratio, H:Q) using traditional peak
22 torque isokinetic measurements has been shown to be a weak risk factor predictor of future lower-limb injuries (e.g.
23 hamstring strain and anterior cruciate ligament tear). In soccer, power-related tasks are commonplace and injuries are
24 most likely to occur during fatigued high-velocity actions. Thus, it is reasonable to that calculating H:Q using power
25 output may serve as an alternative to traditional peak torque-based H:Q. **Aims:** We aimed to investigate the relationship
26 of isokinetic H:Q calculated from traditional peak torque and power output during non-fatigue and fatigue conditions.
27 **Methods:** Seventy-nine professional soccer players (25.6 ± 4.9 years old; 78.7 ± 8.1 kg; 179.4 ± 6.7 cm) performed
28 concentric knee extension-flexion contractions at 60°s^{-1} (5 repetitions) and 300°s^{-1} (30 repetitions, fatigue trial).
29 Traditional peak torque H:Q was calculated using the highest torque obtained during five repetitions at 60°s^{-1} . Power
30 output H:Q_{non-fatigued} was calculated using the average from the 2nd, 3rd and 4th repetitions, and power output H:Q_{fatigued}
31 was obtained as the average of the power output of the last 3 repetitions of the fatigue trial. **Results:** Weak ($r_s=0.27$) and
32 moderate ($r_s=0.49$) correlations were found between traditional peak torque and power output H:Q_{fatigued}, and traditional
33 peak torque and power output H:Q_{non-fatigued}, respectively. **Conclusion:** The present data suggested that power H:Q differ
34 from traditional H:Q, particularly during fatigue in professional soccer players, which warrants further investigation on
35 the potential use of power output H:Q ratios for injury prediction.

36 **Keywords:** muscle strength imbalance; isokinetic strength testing; fatigue; muscle power; football

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39 **Acknowledgments**

40 Filipe Veeck, Rafael Grazioli and Carlos Leonardo Figueiredo Machado are supported by the CAPES PhD
41 scholarship. Ronei Silveira Pinto and Eduardo Lusa Cadore have received a CNPQ (Conselho Nacional de
42 Desenvolvimento Científico e Tecnológico, Brazil) funding. Pedro Lopez is supported by the National Health and Medical
43 Research Council (NHMRC) Centre of Research Excellence (CRE) in Prostate Cancer Survivorship Scholarship. We
44 gratefully acknowledge all organization for the research productivity fellowships.

45

46 **Conflict of interest statement**

47 None to declare.

48

49 **Data availability**

50 Raw data will be available for publisher as requested.

51

52 **Data transparency**

53 All authors make sure that all data and materials as well as software application or custom code support their published
54 claims and comply with field standards.

55

56 **Ethics approval**

57 This study was approved by the Institutional Ethics in Research Committee (protocol number: 2.903.811).

58

59 **Consent to participate**

60 All volunteers agreed to participate through a consent term.

61

62 **Consent for publication**

63 The authors consent with publication in the Sport Sciences for Health.

64

65 **Abbreviations:**

66 **H:Q:** Hamstring to quadriceps ratio

67 **Power output H:Q_{non-fatigued}:** Power output H:Q assessed without fatigue

68 **Power output H:Q_{fatigued}:** Power output H:Q in the fatigued condition

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72 Introduction

73 Power-related tasks such as jumping, and sprinting are essential for soccer performance (Maestroni, 2018). Over
74 the past fifteen years, high-intensity running has increased about 50% in professional soccer matches with elite players
75 increasing the number and distance of sprints by ~35 and 85%, respectively (Barnes et al., 2014). Unfortunately, the
76 incidence of lower-limb injuries such as hamstring strain and knee ligament tears has also been reported (Ekstrand et al.,
77 2011; Erickson et al., 2013). For example, an increase of ~4% and ~6% per year has been reported for hamstring strain
78 and knee ligament tears, respectively (Ekstrand et al., 2011; Rekik et al., 2018), which highlights the need for a more
79 comprehensive injury prevention program and screening strategies (Oakley et al., 2018; Zambaldi et al., 2017).

80 Several approaches have been employed to stratify injury risk and help decision-making about return-to-play in
81 soccer, with isokinetic testing being a common choice (McCall et al., 2014). However, studies by van Dyk et al. (2016),
82 Green et al. (2018) and Dauty et al. (2018) have recently highlighted the low predictive potential value for hamstring and
83 knee ligament tears injuries of traditional isokinetic parameters in soccer players (e.g. peak torque-based hamstring to
84 quadriceps ratio – H:Q). Moreover, since hamstring strain and knee injuries are most likely to occur during high-velocity
85 tasks (Chumanov et al., 2011; Johnston et al., 2018) or in conditions of neuromuscular fatigue (Ekstrand et al., 2011), the
86 traditional peak torque parameters taken from isokinetic tests performed at relatively slow angular velocity (e.g., 60°s^{-1})
87 may not reflect the demands associated with elite soccer performance. As such, new and more ecological approaches are
88 needed to improve injury prediction, prevention, and inform return-to-play decision for professional athletes.

89 Quantification of H:Q based on alternative isokinetic parameters, such as the total work produced in concentric
90 and eccentric knee actions (Minozzo et al., 2018), and during fatigue conditions (Pinto et al., 2017; Lord, Ma'ayah &
91 Blazeovich, 2018) have been shown to differ from peak torque-based H:Q. Accordingly, assessment of isokinetic power
92 output may be an alternative to peak torque for H:Q calculation, as it may reflect more closely the demands of powerful
93 tasks in elite sports (Maestroni, 2018). In addition, the ability to generate force at higher angular speed seems to be more
94 affected by fatigue than peak torque (Buckthorpe et al., 2014; Grazioli et al., 2019), which could be associated to increased
95 risk of injury during power-related tasks. Hence, peak power output derived from isokinetic dynamometry tests (i.e.,
96 product of moment and angular velocity (Iossifidou and Baltzopoulos, 2000)) may be an alternative to traditional H:Q
97 ratios to inform coaches and players about injury risk. However, the relationship between power output and peak torque
98 values on H:Q ratio calculations, as well as the influence of fatigue on such ratios, has been overlooked.

99 Thus, the purpose of the present study was to investigate the relationship of isokinetic H:Q calculated from
100 traditional peak torque and power output during non-fatigue and fatigue conditions. Our hypothesis is that H:Q scores
101 calculated using power output represent a distinct phenomena compared to traditional peak torque H:Q calculations and,
102 hence, will result in distinct and unrelated scores in each athlete.

103 Materials and methods

104 *Participants*

105 Seventy-nine male professional soccer players (25.6 ± 4.9 years old; 78.7 ± 8.1 kg; 179.4 ± 6.7 cm) from three
106 soccer teams playing at national and international levels volunteered for this study. All players were asymptomatic and
107 free from injuries and provided written consent to this study. Tests were performed in both lower limbs during pre-season
108 as part of the players' screening procedure, and data was then retrieved from laboratory database. The regional research
109 ethical committee approved this study (approval number: 2.903.811).

110 *Isokinetic Protocols*

111 Maximal isokinetic knee extension and flexion concentric contractions were performed through a 90° range of
112 motion (0° = full extension) using an isokinetic dynamometer (Cybex Norm, NY, USA). The testing protocol was
113 preceded by a warm-up on a cycle ergometer at comfortable pace for five minutes (Movement Technology, BM2700, SP,
114 Brazil). After that, participants were positioned sitting upright on the dynamometer chair. The lateral epicondyle of the
115 limb was aligned with the dynamometer axis of rotation, and the machine's lever arm was attached to the lower limb, 2
116 cm above the lateral malleolus. Straps were positioned across the participants' thigh, hip and chest to minimize additional
117 movement (Pinto et al., 2017).

118 Prior to testing, the participants performed a specific warm-up consisting of 10 submaximal isokinetic knee
119 extension-flexion repetitions at 120°·s⁻¹. After warm-up, participants performed 5 maximal concentric knee extension-
120 flexion contractions at 60°·s⁻¹ (van Dyk et al. 2016) for baseline peak torque assessment. The power output under non-
121 fatigue and fatigue conditions was assessed during a fatigue trial, which trial consisted of 30 maximal concentric knee
122 extension-flexion repetitions at 300°·s⁻¹, similar to previous studies (Pinto et al., 2017). Athletes were instructed to “push
123 and pull as hard and fast as possible” (Sahaly et al., 2001) and verbal encouragement was given throughout the protocols.
124 There was 90 s of rest between the peak torque and the fatigue trials. Participants were familiar with all testing procedures
125 due to frequent screening routines prior to and during the season. Raw data was exported from the dynamometer software
126 (HUMAC V. 12.17.0, MA, USA) to a personal computer after gravity correction, and peak values of torque and power
127 from both lower limbs were used for further analysis.

128 *Isokinetic protocol analysis*

129 With higher angular velocities (> 180°·s⁻¹), load range phase is shorter and peak moment is likely to occur during
130 the acceleration or deceleration period (Iossifidou and Baltzopoulos, 1996). In this case, moment and angular velocity
131 values are used to calculate power output at high angular velocities (Iossifidou and Baltzopoulos, 2000). Therefore,
132 optimal angular velocities were chosen for each selected variable (i.e., knee extension and flexion peak torque was
133 measured at 60°·s⁻¹, while peak power was assessed at 300°·s⁻¹). Individual H:Q was calculated dividing concentric knee
134 flexion by concentric knee extension performance (i.e. using both peak torque or power, as detailed below).

135 Traditional peak torque H:Q was calculated using the highest torque obtained during five repetitions performed
136 at 60°·s⁻¹. Power output H:Q assessed without fatigue (Power output H:Q_{non-fatigued}) was calculated using the average power
137 output from the 2nd, 3rd and 4th repetitions of the fatigue trial. The 1st repetition was discarded to minimize potential
138 artefacts related to the onset of contraction. Power output H:Q underfatigued condition (H:Q_{fatigued}) was obtained as the
139 average power output of the last 3 repetitions (i.e. 28th, 29th and 30th repetitions) of the fatigue trial.

140 *Statistical analysis*

141 Data normality was assessed using the Shapiro-Wilk test, and descriptive values are shown as mean ± standard
142 deviation (SD) and 95% confidence intervals (95% CI). Independent T-tests were used to compare right and left lower
143 limbs isokinetic values. Since no difference in performance parameters was observed between right and left limb data,
144 both limbs of participants were considered for analysis a single dataset. Paired sample T-test was performed to examine
145 changes in isokinetic performance with the fatigue protocol. Bland-Altman analysis and limits of agreement (±1.96 SDs
146 or the 95% CI) were used to illustrate agreement between measurements and identify bias. A linear regression was used
147 to test for proportional bias. Furthermore, the Spearman's rank-order correlation was employed to assess the relationship

148 between H:Q within the cohort. Finally, traditional peak torque H:Q values were used as an ordinal variable to define
 149 quartiles, and one-way analysis of variance (ANOVA) with Tukey's *post hoc* were used to compare the power output
 150 H:Q_{fatigued} values among quartiles. The level of significance (α) was set at 0.05 and all statistical procedures were
 151 performed using the Statistical Package for Social Science (SPSS) version 20.0 (IBM SPSS Inc., IL, USA).

152 Results

153 *Isokinetic tests performance*

154 No differences were found at baseline between limbs for knee extension (right = 240.6 ± 39.6 ; left = $240.9 \pm$
 155 42.6 N·m, $P = 0.968$) and knee flexion peak torque (right = 148.5 ± 29.5 ; left = 144.9 ± 28.9 N·m, $P = 0.440$). Similarly,
 156 power output did not differ between the right and left limbs during knee extension (right = 354.2 ± 58.9 ; left = $355.6 \pm$
 157 61.0 W, $P = 0.327$) and knee flexion (right = 242.6 ± 52.4 ; left = 233.5 ± 49.9 W, $P = 0.479$). Likewise, no difference
 158 between limbs power output during fatigue was observed for knee extension (right = 220.6 ± 35.5 ; left = 220.3 ± 34.5 W,
 159 $P = 0.811$) and flexion (right = 124.5 ± 35.6 ; left = 121.1 ± 30.4 W, $P = 0.402$). Hence, further analyses were conducted
 160 using the whole sample ($n = 158$ lower limbs). Table 1 describes the comparisons made between different conditions. By
 161 the end of the fatigue protocol, knee extension power output was reduced by 151.3 W (95% CI: -158.6 to -144.0; $P <$
 162 0.001) and knee flexion power output was reduced by 130.6 W (95% CI: -136.8 to -124.4; $P < 0.001$). Power output H:Q
 163 reduced from an average of 0.68 to 0.56 (95% CI: -0.15 to -0.11; $P < 0.001$) with fatigue.

164 Insert Table 1 here

165 *Agreement and correlation between traditional peak torque and power H:Q ratios*

166 Bland-Altman plots showed high agreement between traditional peak torque and both power output H:Q_{non-fatigued}
 167 and power output H:Q_{fatigued}, while a significant proportional bias ($t = 2.31$, $P = 0.022$; Figure 1 panel A) and a non-
 168 significant systematic trend ($t = 0.04$, $P = 0.969$; Figure 1 panel B) were found, respectively. Furthermore, moderate ($r_s =$
 169 0.49 ; $P < 0.001$; Figure 1C) and weak ($r_s = 0.27$; $P < 0.001$; Figure 1D) correlations were found between traditional peak
 170 torque and power output H:Q_{non-fatigued}, and traditional peak torque and power output H:Q_{fatigued}, respectively.

171 Insert Figure 1 here

172 When power output H:Q_{fatigued} was stratified based on athletes traditional peak torque H:Q quartiles (Figure 2),
 173 those with lower peak torque H:Q (i.e. quartile 1) showed lower levels of power output H:Q_{fatigued} when compared to
 174 quartile 3 and 4 ($P = .047$ and $.025$, respectively), while further differences were not found among other quartiles ($P = 0.969$
 175 to 0.997).

176 Insert Figure 2 here

177 Discussion

178 The main purpose of the present study was to examine H:Q derived from peak torque, and power output data
 179 under non-fatigued and fatigued states, and to test the relationship between these measurements. The present findings
 180 showed that, despite the high agreement between them, H:Q derived from peak torque and power output displayed
 181 significant bias and were not strongly associated. Furthermore, while players with the lowest peak torque H:Q also
 182 presented the lowest fatigued power output H:Q, this pattern was not found in players with higher H:Q scores.

183 Previous studies comparing maximal isometric voluntary contraction and rate of torque development (RTD) for
184 calculation of H:Q demonstrated differences in muscle balance imbalance outcomes between ways to calculate H:Q (Zebis
185 et al., 2011; Jordan et al., 2015). Moreover, the disagreement between H:Q calculated with peak torque and alternative
186 methods has been reported to be greater with fatigue in professional soccer players (Grazioli et al., 2019) likely reflecting
187 neural and contractile adjustments to fatigue. For example, Buckthorpe et al. (2014) found faster and more pronounced
188 decline in explosive force than maximal isometric voluntary contraction, which was explained by neural and contractile
189 fatigue mechanisms. Explosive strength is highly dependent on the rate of rise in contractile force at the onset of muscle
190 contraction (Greco et al., 2013), which is likely to be influenced by fibre-type composition (Aagaard et al., 2002). Type
191 II skeletal muscle fibers have a substantially higher RTD (Buckthorpe et al., 2014), and contribute to higher power output
192 (Faulkner et al., 1986). However, type II fibers have lower resistance to fatigue resistance, thus one could expect greater
193 influence of fatigue on explosive compared to maximal force production (Hamada et al., 2003; Buckthorpe et al., 2014).
194 Accordingly, we observed a weak-to-moderate correlation between H:Q derived from traditional peak torque and power
195 output, indicating that maximal force and muscle power production are distinct entities. Furthermore, the dissociation
196 between peak torque and power output was more evident with fatigue in players with higher traditional peak torque H:Q.
197 Given these differences, we speculate that power output H:Q_{fatigued} may be a more ecological measurement as it combines
198 both power-related soccer demands and fatigue in a single test that can be widely used in the athletic population.

199 The dissociation between power output vs. traditional peak torque H:Q becomes even more evident when
200 analyzed beyond correlation results. Quartiles analysis indicated that it is not possible to differentiate the power profiles'
201 in higher quartile players based on their peak torque performance (i.e. athletes with higher traditional peak torque H:Q
202 are not necessarily those displaying the greater power output H:Q_{fatigued} ratio). This result reinforces the differences
203 between maximal strength and power output in non-fatigued and fatigued conditions, respectively. For instance,
204 traditional peak torque H:Q is frequently used by teams to assess the potential power of stabilizing the knee and risk of
205 hamstring strain (McCall et al., 2015). However, based on our results, a player with appropriate traditional peak torque
206 H:Q might well be picked to play, irrespective if his or her H:Q were at low levels if assessed based on fatigued power
207 output tests;

208 The present work analysed a large number of high-level professional soccer players, which strength of this study.
209 Additionally, compared to other rapid force assessment methods (e.g., RTD), which require time-consuming data
210 extraction and analysis (Zebis et al., 2011; Maffiulletti et al., 2016), isokinetic peak power measurement is easily available
211 for medical and strength & conditioning staff, and can be effortlessly retrieved from routine isokinetic tests. However,
212 some limitations are worth noting. Firstly, although all participants were familiar with the assessment protocol, the
213 professional players had limited time for laboratory testing and a test-retest reliability assessment could not be performed.
214 Moreover, the transversal design of this study does not allow us to infer the predictive value of power output H:Q ratios
215 regarding injury risk and whether it could inform decisions about return-to-play. Nevertheless, the current findings
216 provide initial evidence to support further investigation of power output H:Q as an alternative method to traditional muscle
217 imbalance assessment.

218 In conclusion, power output H:Q seems to identify a different muscle balance / imbalance profile compared to
219 traditional peak torque H:Q, especially when fatigue is present. Particularly, in athletes with high peak torque H:Q values,
220 muscle balance calculated based on peak torque and power output were weakly correlated and may not represent the same
221 neuromuscular phenomenon. These findings may provide practitioners with new and more specific information to
222 improve routine screening based on physical demands of soccer. Nevertheless, future prospective cohort studies are

223 needed to investigate whether power-based H:Q could work as an injury prediction variable and serve as a more efficient
 224 screening strategy to inform return-to-play decisions.

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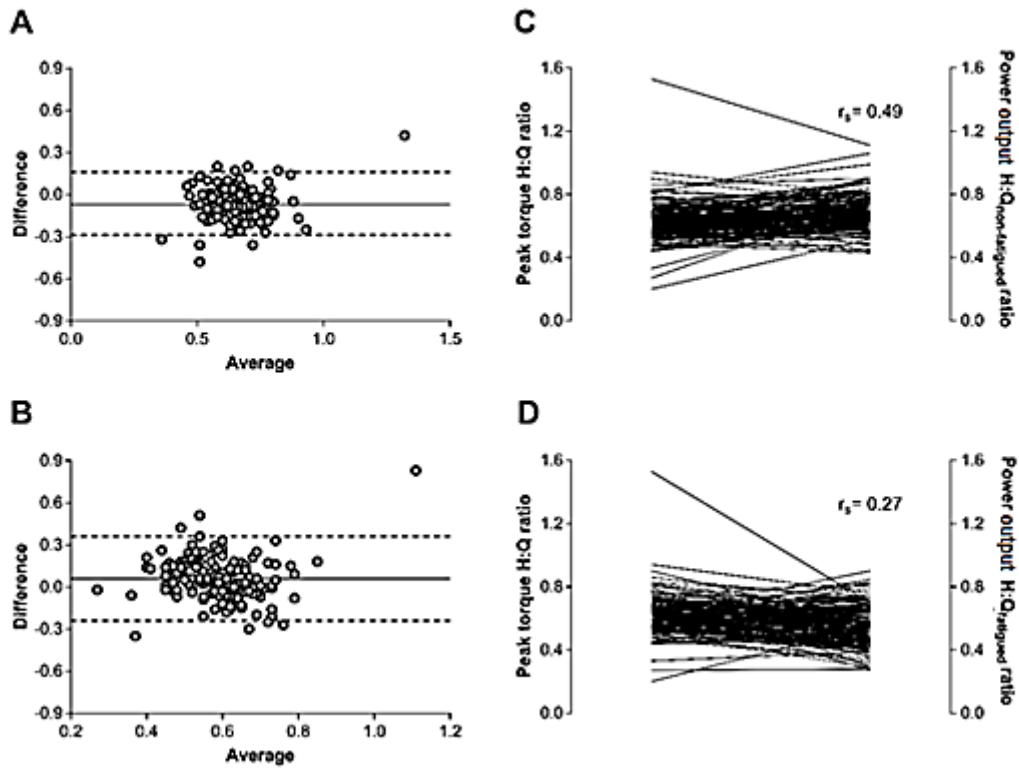
314 **Table 1. Comparisons between peak torque at 60°·s⁻¹ and peak power at 300°·s⁻¹ values in non- and fatigued**
 315 **isokinetic conditions.**

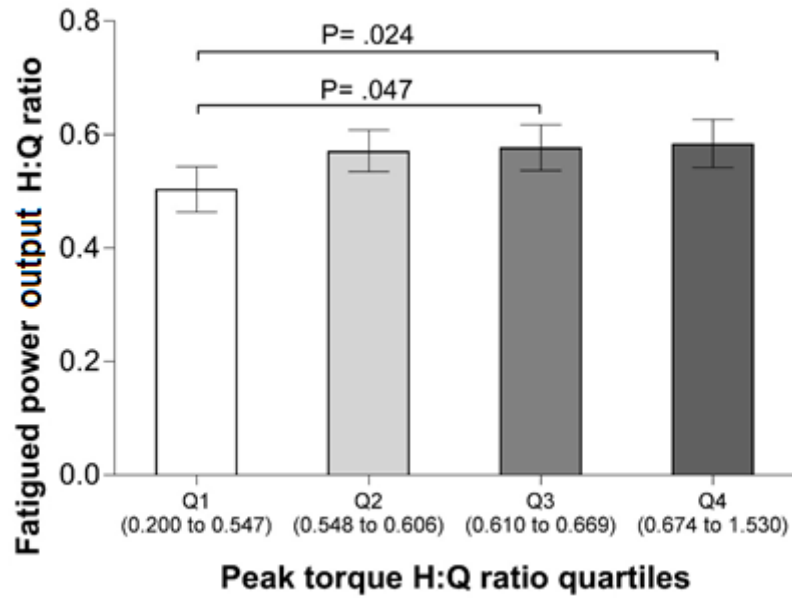
Variable	Non-fatigued Mean ± SD [95% CI]	Fatigued Mean ± SD [95% CI]	Mean difference	95% CI	P-value
Knee extension					
Peak torque at 60°·s ⁻¹ , Nm [†]	240.8 ± 41.0 [234.4 to 247.2]	-	-	-	-
Power at 300°·s ⁻¹ , W	371.7 ± 59.5 [362.4 to 381.0]	220.4 ± 34.9 [215.0 to 225.9]	-151.3	-158.6 to -144.0	<.001
Knee flexion					
Peak torque at 60°·s ⁻¹ , Nm [†]	146.7 ± 29.1 [142.1 to 151.2]	-	-	-	-
Power at 300°·s ⁻¹ , W	253.4 ± 51.6 [245.4 to 261.5]	122.8 ± 33.0 [117.7 to 128.0]	-130.6	-136.8 to -124.4	<.001
H:Q					
Peak torque at 60°·s ^{-1†}	0.62 ± 0.12 [0.60 to 0.64]	-	-	-	-
Power at 300°·s ⁻¹	0.68 ± 0.11 [0.67 to 0.70]	0.56 ± 0.13 [0.54 to 0.58]	-0.12	-0.15 to -0.11	<.001

316 *SD = standard deviation; CI = confidence interval; †, Test not performed under fatigue; H:Q, hamstring-to-quadriceps*
 317 *ratio.*

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319 **Figure 1.** Bland-Altman plots of traditional peak torque, power output $H:Q_{non-fatigued}$ (A) and power output $H:Q_{fatigued}$
320 values (B), and correlation between individual scores in traditional peak torque, power output $H:Q_{non-fatigued}$ (C) and
321 power output $H:Q_{fatigued}$ values (D).
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Figure 2. Absolute values and 95% confidence intervals of fatigued power output H:Q values according to traditional peak torque H:Q quartiles. Quartile 1 (Q1) lowest traditional peak torque H:Q values to quartile 4 (Q4) highest traditional peak torque H:Q values. Traditional peak torque H:Q cut-points were 0.548 for Q2, 0.610 for Q3, and 0.674 for Q4. The P-value is for comparisons between quartiles